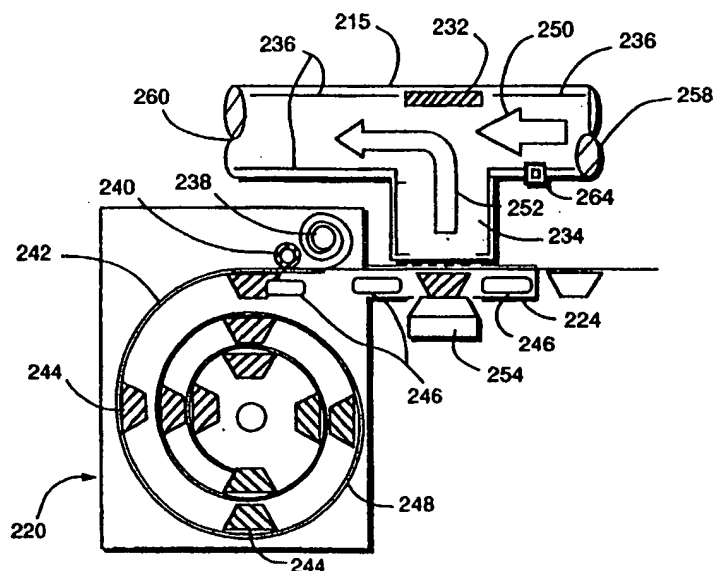




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(54) Title: INHALATION DEVICE



## (57) Abstract

An inhaler (220) that utilizes vibration to facilitate suspension of powder into an air stream is provided. One embodiment of the inhaler includes a piezoelectric vibrator (254) for vibrating the powder. A controller is provided for controlling supply of actuating electricity to the vibrator so as to cause the powder to vibrate in such a way as to deaggregate the powder and separate the powder by size. The powder particles of interest are then suspended in the air stream by electrostatic means (232).

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## INHALATION DEVICE

The present invention relates generally to the field of inhalation devices, and more specifically, to inhalation devices that utilize vibration to facilitate suspension of powder (e.g., powdered medication) into an inhaled gas stream (e.g., of inhaled air). Particular utility for the present invention is found in the area of facilitating inhalation of powdered medications (e.g., bacterial vaccines, sinusitis vaccines, antihistaminic agents, vaso-constricting agents, anti-bacterial agents, anti-asthmatic agents, theophylline, aminophylline, di-sodium cromolyn, etc.), although other utilities are contemplated, including other medicament applications.

Certain diseases of the respiratory tract are known to respond to treatment by the direct application of therapeutic agents. As these agents are most readily available in dry powdered form, their application is most conveniently accomplished by inhaling the powdered material through the nose or mouth. This powdered form results in the better utilization of the medicament in that the drug is deposited exactly at the site desired and where its action may be required; hence, very minute doses of the drug are often equally as efficacious as larger doses administered by other means, with a consequent marked reduction in the incidence of undesired side effects and medicament cost. Alternatively, the drug in this form may be used for treatment of diseases other than those of the respiratory system. When the drug is deposited on the very large surface areas of the lungs, it may be very rapidly absorbed into the blood stream; hence, this method of application may take the place of administration by injection, tablet, or other conventional means.

It is the opinion of the pharmaceutical industry that the bioavailability of the drug is optimum when the drug particles delivered to the respiratory tract are between 1 to 5 microns in size. When the drug particles need to be in this size range the dry powder delivery system needs to address a number of issues:

(1) Small size particles develop an electrostatic charge on themselves during manufacturing and storage. This causes the particles to agglomerate or aggregate, resulting in clusters of particles which have an effective size greater than 5 microns. The probability of these large clusters making it to the deep lungs then decreases.

1 This would result in a lower percentage of the packaged drug being available to the  
2 patient for absorption.

3 (2) The amount of active drug that needs to be delivered to the patient may be  
4 of the order of 10s of micrograms. For example, albuterol, in the case of a drug used  
5 in asthma, this is usually 25 to 50 micrograms. Current manufacturing equipment can  
6 effectively fill milligrams of drug with acceptable accuracy. So the standard practice  
7 is to mix the active drug with a filler or bulking agent such as lactose. This additive  
8 also makes the drug "easy to flow". This filler is also called a carrier since the drug  
9 particles also stick to these particles through electrostatic or chemical bonds. These  
10 carrier particles are very much larger than the drug particles in size. The ability of the  
11 dry powder inhaler to separate drug from the carrier is an important performance  
12 parameter in the effectiveness of the design.

13 (3) Active drug particles with sizes greater than 5 microns will be deposited  
14 either in the mouth or throat. This introduces another level of uncertainty since the  
15 bioavailability and absorption of the drug in these locations is different from the  
16 lungs. Dry powder inhalers need to minimize the drug deposited in these locations to  
17 reduce the uncertainty associated with the bio-availability of the drug.

18 Prior art dry powder inhalers (DPIs) usually have a means for introducing the  
19 drug (active drug plus carrier) into a high velocity air stream. The high velocity air-  
20 stream is used as the primary mechanism for breaking up the cluster of micronized  
21 particles or separating the drug particles from the carrier. Several inhalation devices  
22 useful for dispensing this powder form of medicament are known in the prior art. For  
23 example, in U.S. Patent Nos. 3,507,277; 3,518,992; 3,635,219; 3,795,244; and  
24 3,807,400, inhalation devices are disclosed having means for piercing of a capsule  
25 containing a powdered medicament, which upon inhalation is drawn out of the pierced  
26 capsule and into the user's mouth. Several of these patents disclose propeller means,  
27 which upon inhalation aid in dispensing the powder out of the capsule, so that it is not  
28 necessary to rely solely on the inhaled air to suction powder from the capsule. For  
29 example, in U.S. Patent No. 2,517,482, a device is disclosed having a powder  
30 containing capsule placed in a lower chamber before inhalation, where it is pierced by

1 manual depression of a piercing pin by the user. After piercing, inhalation is begun  
2 and the capsule is drawn into an upper chamber of the device where it moves about in  
3 all directions to cause a dispensing of powder through the pierced holes and into the  
4 inhaled air stream. U.S. Patent No. 3,831,606 discloses an inhalation device having  
5 multiple piercing pins, propeller means, and a self-contained power source for  
6 operating the propeller means via external manual manipulation, so that upon  
7 inhalation the propeller means aids in dispensing the powder into the stream of  
8 inhaled air. See also U.S. Patent No. 5,458,135.

9 These prior art devices present several problems and possess several  
10 disadvantages which are remedied by the inhalation devices of the present invention.  
11 For instance, these prior art devices require that the user exert considerable effort in  
12 inhalation to effect dispensing or withdrawal of powder from a pierced capsule into  
13 the inhaled air stream. With these prior art devices, suction of powder through the  
14 pierced holes in the capsule caused by inhalation generally does not withdraw all or  
15 even most of the powder out of the capsule, thus causing a waste of the medicament.  
16 Also, such prior art devices result in uncontrolled amounts or clumps of powdered  
17 material being inhaled into the user's mouth, rather than a constant inhalation of  
18 controlled amounts of finely dispersed powder.

19 The above description of the prior art is taken largely from U.S. Pat. No.  
20 3,948,264 to Wilke et al, who disclose a device for facilitating inhalation of a  
21 powdered medication that includes a body portion having primary and secondary air  
22 inlet channels and an outlet channel. The secondary inlet channel provides an  
23 enclosure for a capsule containing the powdered medication and the outlet channel is  
24 formed as a mouthpiece protruding from the body. A capsule piercing structure is  
25 provided, which upon rotation puts one or more holes in the capsule so that upon  
26 vibration of the capsule by an electro-mechanical vibrator, the powdered drug may be  
27 released from the capsule. The piercing means disclosed in Wilke et al includes three  
28 radially mounted, spring-biased piercing needles mounted in a trochoidal chamber.  
29 Upon hand rotation of the chamber, simultaneous inward radial motion of the needles  
30 pierces the capsule. Further rotation of the chamber allows the needles to be retracted

1 by their spring mountings to their original positions to withdraw the needles from the  
2 capsule. The electromechanical vibrator includes, at its innermost end, a vibrating  
3 plunger rod which projects into the intersection of the inlet channel and the outlet  
4 channel. Connected to the plunger rod is a mechanical solenoid buzzer for energizing  
5 the rod to vibrate. The buzzer is powered by a high energy electric cell and is  
6 activated by an external button switch. According to Wilke et al, upon inhalation  
7 through outlet channel 3 and concurrent pressing of switch 10d to activate the  
8 electromechanical vibrating means 10, air is sucked through inlet channels 4 and 12  
9 and the air stream through the secondary inlet channel 4 raises the capsule up against  
10 the vibrating plunger rod 10a. The capsule is thus vibrated rapidly with powder being  
11 fluidized and dispensed from the pierced holes therein. (This technique is commonly  
12 used in manufacturing for dispensing powder through a hopper where the hopper is  
13 vibrated to fluidize the powder and move it through the hopper outlet. The pierced  
14 holes in the capsule represent the hopper outlet.) The air stream through inlet channel  
15 4 and 12 aids in withdrawal of powder from the capsule and carries this powder  
16 through the outlet channel 3 to the mouth of the user." (Wilke et al, column 3, lines  
17 45-55). Wilke et al further discloses that the electromechanical vibrator means may  
18 be placed at a right angle to the inlet chamber and that the amplitude and frequency of  
19 vibration may be altered to regulate dispensing characteristics of the inhaler.

20 Thus, as noted above, the vibrator in Wilke et al's disclosed inhaler is an  
21 electromechanical device consisting of a rod driven by a solenoid buzzer. (This  
22 electromechanical means may be a motor driving a cam [Col. 4, Line 40]). A  
23 disadvantage of the inhaler implementation as disclosed by Wilke is the relatively  
24 large mechanical movement required of the rod to effectively vibrate the capsule. The  
25 large movement of the rod, usually around 100s of microns, is necessary due to the  
26 elasticity of the capsule walls and inertia of the drug and capsule.

27 Moreover, solenoid buzzers typically have operating frequencies less than 5  
28 Khz. This operating frequency tends to be noisy and therefore is not desirable when  
29 incorporated into a dry powder inhaler from a patient's perspective. A further  
30 disadvantage of the electrochemical actuators of Wilke is the requirement for a high

1 energy source (Wilke et al, Col. 3, line 38), thus requiring a large battery source or  
2 frequent changes of the battery pack for portable units. Both these features are not  
3 desirable from a patient safety and "ease of use" standpoint.

4 The inhaler of Wilke et al is primarily intended to reduce the amount of  
5 powder left behind in the capsule relative to other inhalers cited in the patent  
6 disclosure. (Wilke et al, Col. 4, lines 59-68, Col. 5, lines 1-48). However, Wilke et al  
7 does not address the need to deaggragate the powder into particle sizes or groups less  
8 than 6 microns in size as is required for effective delivery of the medication to the  
9 lungs; rather Wilke et al, like the prior art inhalers continues to rely on the air stream  
10 velocity to deaggregate the powder ejected into the air stream, into particle sizes  
11 suitable for delivery to the lungs.

12 Another prior art inhalation device is disclosed in Burns et al U.S. Patent No.  
13 5,284,133. In this device, a liquid medication is atomized by an ultrasonic device  
14 such as a piezo element (Burns et al, Col. 10, lines 36-51). A stream of air, usually at  
15 a high velocity, or a propellant then carries the atomized particles to the patient. The  
16 energy required to atomize the liquid medication in the nebulizer is prohibitively high,  
17 making this approach for the delivery of drugs to the lungs only feasible as a desk top  
18 unit. The high voltage requirements to drive the piezo, to produce the necessary  
19 mechanical displacements, also severely effects the weight and size of the device. It  
20 is also not obvious that the nebulizer operating principles can be applied to the dry  
21 powder inhalers for delivery or powder medication to the lungs.

22 The prior art devices therefore have a number of disadvantages which makes  
23 them less than desirable for the delivery of dry powder to the lungs. Some of these  
24 disadvantages are:

- 25 • The performance of the prior art inhalers depends on the flowrate  
26 generated by the user. Lower flowrate does not result in the powder being  
27 totally deaggregated and hence adversely affects the dose delivered to the  
28 patient.
- 29 • Inconsistency in the bioavailability of the drugs from dose-to-dose because  
30 of lack of consistency in the deaggregation process.

- 1           • Large energy requirements for driving the electromechanical based  
2           inhalers which increases the size of the devices making them unsuitable for  
3           portable use.

4           Thus, it is the general object of the present invention to provide an inhaler that  
5           utilizes vibration to facilitate suspension of powder into a gas that overcomes the  
6           aforesaid and other disadvantages and drawbacks of the prior art. Accordingly, one  
7           embodiment of the inhaler of the present invention includes a piezoelectric vibrator  
8           for vibrating the powder. A controller is provided for controlling supply (i.e.,  
9           amplitude and/or frequency) of actuating electricity to the vibrator so as to cause  
10          vibration of the powder that is adapted to optimally suspend at least a portion of the  
11          powder into the gas. In this embodiment of the present invention, the controller may  
12          include a user-actuable control for permitting the user to select the vibration  
13          frequencies and/or amplitudes for optimally suspending in the gas the type of powder  
14          currently being used in the inhaler. The user-actuable control is pre-calibrated with  
15          the controller to cause the controller to adjust the frequency and/or amplitude of  
16          actuating electricity supplied to the vibrator to be that necessary for vibrating the type  
17          of powder selected by the user-actuable control in such a way as to optimally suspend  
18          at least a portion of the powder into the gas. The user-actuable control may include  
19          selection gradations in terms of the average size of the powder particles to be  
20          suspended in the gas, and/or in terms of desired vibration frequencies and amplitudes.  
21          Typically, for commonly used powdered medications of 0.5 to 10 micron size, more  
22          typically 1 to 5 micron size, vibration frequency would be adjusted to at least about 12  
23          KHz, in order to optimally suspend such commonly used powdered medications in the  
24          gas. Of course, vibration frequency and amplitude may be adjusted to optimize  
25          suspension of the powdered medication being used.

26          Advantageously, the piezoelectric vibrator in this embodiment of the invention  
27          does not include the many moving mechanical parts of prior art electromechanical  
28          vibrator in the inhalers such as disclosed in Wilke et al. Thus, the vibrator in this  
29          embodiment does not require the frequent maintenance required by vibrator devices  
30          such as disclosed in Wilke et al. Further advantageously, the controller and user-



1    actuable control of this embodiment of the present invention permit the vibration  
2    amplitude and frequency imparted to the powder to be quickly and easily adjusted for  
3    optimal delivery of different types of powders to the user without the inconvenience  
4    of having to disassemble and alter the physical components of this embodiment.

5            A second embodiment of the invention includes a controllable vibrator for  
6    vibrating the powder and a controller for controlling the vibrator. The controller  
7    controls the vibrator based, at least partially, upon at least one detected characteristic  
8    of the user's inhalation gas stream in and through the inhaler. The detected  
9    characteristics of the gas stream upon which the controller bases its control of the  
10   vibrator may include the detected velocity, flowrate, and/or pressure of the inhalation  
11   gas stream. The vibrator in this second embodiment may comprise a piezoelectric  
12   vibrator. Additionally, the controller of this second embodiment may control the  
13   vibrator by automatically actuating the vibrator when the at least one detected  
14   characteristic of the gas stream has a magnitude that exceeds a minimum threshold  
15   value therefor indicative of inhalation by the user, and by automatically deactivating  
16   the vibrator when the magnitude of the at least one detected characteristic is less than  
17   the minimum threshold.

18           This second embodiment may also include a plurality of gas inlets and at least  
19   one one-way valve in at least one of the inlets. The valve is adapted to permit flow of  
20   gas into the inhaler therethrough upon inhalation of gas from the inhaler.

21           This second embodiment may also include a dispenser for dispensing the  
22   powder for being vibrated. The dispenser dispenses the powder based upon control  
23   signals supplied to the dispenser by the controller. The controller generates these  
24   control signals based upon, at least in part, the at least one detected characteristic of  
25   the gas stream. The dispenser may dispense the powder directly to the surface of the  
26   vibrator.

27           Advantageously, these features of this second embodiment permit this  
28   embodiment to be able to commence dispensing and vibration of the powder  
29   simultaneously with inhalation by the user. Additionally, the one-way valve of this  
30   second embodiment prevents outflow of powder from the inhaler unless except during

1 inhalation by the user. These features permit the powdered medication to be  
2 delivered to the user with much less waste and with a greater degree of dosage control  
3 than is possible according to the prior art.

4 In a third embodiment of the invention, a vibrator is provided for vibrating the  
5 powder. A controller is provided for controlling supply (i.e., frequency and/or  
6 amplitude) of actuating electricity to the vibrator based, at least in part, upon detected  
7 power transfer characteristics of the vibrator. Preferably, in this third embodiment,  
8 the detected power transfer characteristics upon which the controller bases its control  
9 of the supply of power include whether the maximum power is being transferred to  
10 the vibrator. The controller automatically adjusts the supply of power to the vibrator  
11 so as to maximize the detected power transferred to the vibrator.

12 Advantageously, it has been found that the powder is optimally suspended in  
13 the gas when detected power transferred to the vibrator is maximized. Thus, by  
14 utilizing the aforesaid automatic feedback and control features of this third  
15 embodiment of the present invention, the powder may be optimally suspended in the  
16 gas with little to no user interaction with the inhaler (i.e., the user does not need to  
17 adjust the frequency and/or amplitude of vibration himself).

18 Another embodiment of the inhaler of the present invention includes a  
19 piezoelectric vibrator for vibrating the drug, which may be a pure micronized drug or  
20 a micronized drug on a carrier, in a container such as a blister pack so as to  
21 deaggregate clumps of the drug or separate the micronized drug from the carrier  
22 particles. Since the intent of the invention is to ensure consistency in the  
23 bioavailability of the drug from dose-to-dose, the amount of energy coupled into the  
24 powder is sufficient to cause deaggregation to happen and maintain the powder in a  
25 fluidized state, but is not so high as to prematurely eject clumps of powder into the air  
26 stream that is flowing across the blister.

27 In yet another embodiment, a vibrator having a vibrating diaphragm is  
28 provided for imparting vibrations to the powder. The vibrator may include  
29 electrostatic, electromagnetic, or magnetostrictive means for rapidly deflecting the  
30 diaphragm. The magnetostrictive means uses at least one ferromagnetic member

1 adapted to change its dimensions and/or shape in the presence and as a function of the  
2 magnetic flux applied to the member by a magnetic flux generating means. The  
3 magnetic flux generating means may comprise a permanent magnet and a coil, or an  
4 electromagnetic means for generating and applying the magnetic flux to the  
5 ferromagnetic member.

6 The micronized particle sizes of interest are then lifted out of the fluidized  
7 powder by the passing air stream. In a preferred embodiment of the invention, an  
8 electrostatic field that is established across the air stream. By controlling the strength  
9 of the electrostatic field only particle sizes of interest are introduced into the air  
10 stream. The larger size particles are left behind in the container. This reduces the  
11 inconsistency associated with the bioavailability of the drug because of the large  
12 particles being deposited into the mouth or throat as is common with devices  
13 described in prior art.

14 Reference is made to the drawings, wherein like numerals depict like parts,  
15 and wherein:

16 Figure 1 is a perspective view of one embodiment of the inhaler of the present  
17 invention.

18 Figure 2 is a rear plane view of the inhaler shown in Figure 1.

19 Figure 3 is a longitudinal cross-sectional schematic view of the preferred  
20 embodiment of Figure 1.

21 Figure 4 is a functional block diagram of the vibration control system of the  
22 embodiment of Figure 1.

23 Figure 5 is a perspective view of a second preferred embodiment of the inhaler  
24 of the present invention.

25 Figure 6 is a functional block diagram of the vibration control system of the  
26 embodiment of Figure 5.

27 Figure 7A and 7B are side elevations of another embodiment of an inhaler of  
28 the present invention;

29 Figure 8 is an end view of the embodiment of Figure 7;

1        Figures 9A and 9B is an enlarged cross-sectional views of the embodiment of  
2        Figure 7;

3        Figure 10 is a functional schematic diagram of the electrical/electronic system  
4        used in the inhaler of Figure 7;

5        Figure 11 is a schematic representation of a preferred vibrator driver circuit  
6        used for exciting the piezoelectric vibrator;

7        Figures 12A and 12B are schematic representations of the electrostatic voltage  
8        generation circuit used in the inhaler of Figure 7; and

9        Figure 13 is a view similar to Figure 9A, and showing yet another embodiment  
10       of the present invention.

11       Referring to Figures 1-4, one preferred embodiment 10 of the inhaler of the  
12       present invention will now be made. Inhaler 10 includes a hard plastic or metal  
13       housing 18 having a generally L-shaped longitudinal cross-section. Housing 18  
14       includes four air flow openings 20, 28, 30, and 32 (whose function in this embodiment  
15       of inhaler 10 of the present invention will be described more fully below). Inhaler 10  
16       includes a main air flow passage 26 which extends the length of the housing 18 from  
17       the front 22 (at opening 20) to the rear 24 thereof (at opening 28) and has a generally  
18       square-shaped transverse cross-section, so as to permit air flow therethrough (denoted  
19       by arrow F in Figure 1).

20       Secondary air conduit 31 is generally L-shaped and runs longitudinally from  
21       opening 30 in the rear 24 surface of the housing 18 to main passage 26. One-way  
22       flow valve 50 is mounted to the inner surface 33 of the main passage 26 via a  
23       conventional spring-biased hinge mechanism (not shown), which is adapted to cause  
24       the valve 50 to completely block air flow S through the conduit 31 to the main  
25       passage 26 when the pressure of the air flow F in the main passage 26 is below a  
26       predetermined threshold indicative of inhalation through the passage 26 by a user.

27       Powder dispensing chamber 51 is formed in housing 18 for holding a capsule  
28       34 of powder medication to be inhaled. Housing 18 includes a moveable panel  
29       portion 32 in the rear 24 for permitting the capsule 34 to be introduced into the  
30       chamber 51 and placed on the seating 52 of vibration means 36 between guiding

1 means 60A, 60B. Preferably, means 36 comprises a hard plastic or metallic protective  
2 shell 37 enclosing a piezoelectric vibrator 90. Preferably, vibrator 90 is mechanically  
3 coupled through the shell 37 via a disk (not shown) to the drug cartridge 34 so as to  
4 permit maximum vibratory energy to be transmitted from the vibrator 90 through the  
5 shell 37 to the cartridge 34. Guiding means 60A, 60B includes two surfaces which  
6 slant downwardly toward the seating 52 so as to permit easy introduction and  
7 retention of the capsule on the seating 52 in the chamber 51. Removable panel 32  
8 includes another air inlet 34 for permitting additional air flow S2 from the chamber 51  
9 through conduit 61 into conduit 31 during inhalation by the user. Preferably, panel  
10 32 and housing 18 include conventional mating mounting means (not shown) for  
11 permitting the panel 32 to be removably resecurable to the housing by the user  
12 between introduction of fresh (i.e., completely full) capsules and removal of spent  
13 (i.e., empty) capsules.

14 Inhaler 10 also includes a conventional miniature air stream velocity or  
15 pressure sensor 40 mounted on the inner surface of the conduit 26 so as to sense the  
16 speed and/or pressure of the air stream F. Preferably, sensor 40 comprises a  
17 conventional spring-loaded flapper-yield switch which generates electronic signals  
18 indicative of the speed and/or pressure of the air stream F in the conduit 26, and  
19 transmits those signals via electrical connection 42 to electronic control circuitry 48  
20 contained in housing 18 for controlling actuation of the vibrator means based upon  
21 those signals.

22 Preferably, the control circuitry 48 is embodied as an application specific  
23 integrated circuit chip and/or some other type of very highly integrated circuit chip.  
24 As will be described more fully below, the control circuitry 48 determines the  
25 amplitude and frequency of actuating power to be supplied from conventional power  
26 source 46 (e.g., one or more D.C. batteries) to the piezoelectric vibrator to thereby  
27 control vibration of the vibrator. The actuating power is supplied to the piezoelectric  
28 element 90 via electrical connection 44 between the vibrator and the circuitry 48.

29 Piezoelectric element 90 is made of a material that has a high-frequency, and  
30 preferably, ultrasonic resonant vibratory frequency (e.g., about 15 to 50 kHz), and is

1 caused to vibrate with a particular frequency and amplitude depending upon the  
2 frequency and/or amplitude of excitation electricity applied to the piezoelectric  
3 element 90. Examples of materials that can be used to comprise the piezoelectric  
4 element 90 include quartz and polycrystalline ceramic materials (e.g., barium titanate  
5 and lead zirconate titanate). Advantageously, by vibrating the piezoelectric element  
6 90 at ultrasonic frequencies, the noise associated with vibrating the piezoelectric  
7 element 90 at lower (i.e., non-ultrasonic) frequencies can be avoided.

8 Turning to Figure 4, the various functional components and operation of the  
9 control circuitry 48 will now be described. As will be understood by those skilled in  
10 the art, although the functional components shown in Figure 4 are directed to an  
11 analog realization of the control circuitry 48, the components of Figure 4 could be  
12 appropriately modified to realize control circuitry 48 in a digital embodiment without  
13 departing from this embodiment 10 of the present invention.

14 Control circuitry 48 preferably includes actuation controller 70 and vibratory  
15 feedback control system 72. Actuation controller 70 comprises a conventional  
16 switching mechanism for permitting actuating power to be supplied from the power  
17 source 46 to the control system 72 depending upon the signals supplied to it from  
18 sensor 40 and the state of the power switch 12. In other words, controller 70 permits  
19 actuating power to be supplied from the source 46 to the system 72 when the sliding  
20 indicator bar 14 of switch 12 is set to the "ON" position in channel track 16 and the  
21 inhalation sensor 40 supplies signals to the controller 70 that indicate that the  
22 inhalation is occurring through the main passage 26. However, controller 70 does not  
23 permit actuating power to flow from the source to the system 72 when either the  
24 switch 12 is set to "OFF" or the signals supplied to the controller 70 from the sensor  
25 40 indicate that inhalation is not taking place through the conduit 26.

26 When controller 70 first permits actuating power to be supplied from the  
27 source 46 to the feedback control system 72, the system 72 enters an initialization  
28 state wherein controllable means for supplying a predetermined frequency and  
29 amplitude of actuating electricity 74 is caused to generate control signals for causing  
30 conventional pump circuit 80 to generate an initial desired frequency and amplitude of

1 actuating electricity based upon stored values thereof stored in the initialization  
2 memory means 82. Preferably, means 74 comprises conventional frequency sweep  
3 generator and frequency generator means 76 and 78, respectively. The signals  
4 generated by means 74 are then supplied to charge pump circuit 80 to cause circuit 80  
5 to supply the piezoelectric element 90 with actuating electricity specified by the  
6 signals.

7        Preferably, the initial frequency and amplitude of actuating electricity  
8 supplied to the piezoelectric element 90 is pre-calibrated to cause the piezoelectric  
9 element 90 to vibrate at its resonance frequency when no powder cartridge or powder  
10 is placed on the means 36. As will be appreciated by those skilled in the art,  
11 maximum transfer of vibratory power from the piezoelectric element to the powder in  
12 the container 34 takes place when the piezoelectric element vibrates at its resonant  
13 frequency. It has been found that this results in maximum de-aggregation and  
14 suspension of the powder from the container 34 into the air to be inhaled by the user.  
15 However, when the container 36 or powder is placed on the vibrator means 36, the  
16 weight and volume of the powder container, and the weight, volume, and particular  
17 size of the powder to be suspended by the piezoelectric element can change the  
18 vibration characteristics of the piezoelectric element, and cause the piezoelectric  
19 element to vibrate at other than its resonant frequency. This can result in reduced  
20 vibratory energy transfer to the powder from the piezoelectric element, and thereby,  
21 lessen the efficiency of the piezoelectric element in de-aggregating and suspending the  
22 powder in the air inhaled by the user.

23        The feedback control system 72 of the present invention overcomes this  
24 problem. In control system 72, after the initial frequency and amplitude of actuating  
25 electricity are supplied to the piezoelectric element 90, the frequency generating  
26 means 74 systematically generates control signals indicative of many different  
27 amplitudes and frequencies of electricity for being supplied to the piezoelectric element  
28 90 by the circuit 80. As the generating means 74 "cycles through" the different  
29 frequencies and amplitudes, the instantaneous power transfer characteristics of the  
30 piezoelectric element 90 for each of these different frequencies and amplitudes are

1 determined by the detector 88, which transmits this information to the peak power  
2 detector 86. Peak detector 86 analyzes the instantaneous power transfer  
3 characteristics of the piezoelectric element 90 and signals the sample and hold  
4 feedback controller 84 when the power transfer characteristics are at local maxima.  
5 The controller 84 correlates these local maxima with the frequencies and amplitudes  
6 commanded by the generator 74 to be supplied to the piezoelectric element 90.

7 After the frequency generator 74 has finished its sweep through the  
8 frequencies and amplitudes of power supplied to the piezoelectric element 90, the  
9 controller 84 causes the generator 74 to cycle through the frequencies and amplitudes  
10 of power that resulted in local maxima, and then determines which of these  
11 frequencies and amplitudes results in optimal power transfer characteristics through  
12 the piezoelectric element 90.

13 In operation of embodiment 10, the drug-containing package 34 is punctured  
14 and inserted onto the surface 52 of vibrator 36 in chamber 51 in the manner described  
15 previously. The power switch is placed in the "ON" position and the user inhales air  
16 through the conduit 26, air flow F is generated through conduit 26. This causes one-  
17 way valve 50 to deflect to admit air flow S through opening 30 into conduit 26, and  
18 also causes air flow S2 through opening 34 and chamber 51 into conduit 26. The  
19 inhalation of air stream F is sensed by sensor 40 and is signaled to actuation controller  
20 70, which causes power to be supplied to the controller 72. The controller 72 then  
21 adjusts the amplitude and frequency of actuating power supplied to the piezoelectric  
22 element until they are optimized for the best possible de-aggregation and suspension  
23 of the powder P from the capsule into the air stream F via air flows S and S2.

24 Turning to Figures 5-6, a second preferred embodiment 100 of the present  
25 invention will now be described. It should be appreciated that unless specifically  
26 indicated to the contrary, the components and operation of embodiment 100 are  
27 substantially identical to those of embodiment 10. In embodiment 10, the feedback  
28 controller 72 of embodiment 10 is replaced with a pre-calibrated controller 112.  
29 Controller 112 includes precalibrated frequency/amplitude control signal generator  
30 110 which supplies control signals to pump circuit 80 based upon signals supplied to



1 it from user-actuable frequency/amplitude controller switch 102. Switch 102 includes  
2 indicator means 106 slidably mounted in channel track 108 and permits a user to  
3 command the generator 110 to generate control signals for causing the pump 80 to  
4 supply amplitude and frequencies of actuating power to the piezoelectric element for  
5 optimally suspending powders of differing, pre-calibrated particular sizes. For  
6 example, when the selector switch is set to the "1-5" position, the generator 110 may  
7 be pre-programmed to generate control signals for causing the pump 80 to supply to  
8 the piezoelectric element 90 actuating electricity having a frequency and amplitude for  
9 optimally suspending powder particles between about 1 and 5 microns in size. Of  
10 course, it will be appreciated that the pre-calibrated optimal frequency and amplitude  
11 values programmed in generator 110 are based upon an expected weight and volume  
12 of the container 34 and powder contained therein. Thus, in order for the inhaler 100 to  
13 be able to optimally suspend the powder, the weight and volume of the container 34  
14 and powder contained therein cannot differ significantly from the expected values  
15 thereof upon which the pre-calibration values programmed into the generator 110  
16 were based.

17 Referring to Figures 7-12, another and preferred embodiment 200 of the  
18 inhaler of the present invention will now be described. The inhaler 200 comprises a  
19 housing 212 having a mouthpiece 214 at one end of leg 215 thereof, and an air inlet  
20 opening 216 at the opposite end of the same leg 215. The leg 215 forms a hollow  
21 channel that is unobstructed between the opening 214 and 216. Referring in particular  
22 to Figure 9A, a passageway 234 is formed in leg 215 intermediate of mouthpiece 214  
23 and inlet 216. This passageway communicates with a drug cartridge 220. Opposite  
24 this passageway 234 is a high frequency piezoelectric 254 vibrator located in member  
25 226 of the inhaler housing 212. An inhalation sensor 264 is also located between the  
26 passageway 234 and the inlet 216 of the inhaler.

27 Disposable cartridge 220 comprises an outer housing 222 which includes a tab  
28 224 for slidably mounting in recess 218 formed integrally to the housing 212. Drug  
29 cartridge 220 includes a coiled tape 248 carrying a plurality of spaced blisters or wells  
30 244 for carrying a dry powder medicament. A release film 242 covers and seals wells

1 244. Tape 248 is formed as a coil, and threaded between guide platen 246 and pinch  
2 roller 240. Pinch roller 240 is driven by a take-up spool 238 which in turn is driven  
3 by the thumbwheel 230. In use, as the thumbwheel 230 is turned, it peels the release  
4 film 242 from the tape 248 to expose the wells 244 carrying the drug, and the release  
5 film is collected by the take-up spool 238. This collection of the release film  
6 advances a new well carrying the drug over the piezoelectric vibrator 254 housed in  
7 location 226 of the inhaler housing 215. Tape 248 also preferably includes detent  
8 means or the like for indexing the tape so a selected well 244 is automatically  
9 positioned over the piezoelectric element 254.

10 Referring to Figure 9A, a passageway 234 allows the selected well 244 to  
11 communicate with the hollow channel 215. Passageway 234 should be of sufficient  
12 length to serve the purpose of avoiding to introduce the drug prematurely into the air  
13 stream 250, which could be zero, if the wells 244 have sufficient depth. Above the  
14 exposed well 244, in the passageway 234, is an electrostatic plate 232 on the inside  
15 wall of the hollow channel 215. Channel 215 also includes an inhalation sensor 264,  
16 the purpose of which is to detect the flow of an air stream from the inlet 216 to the  
17 mouthpiece 214. This sensor signal is used to sequence the electronic control of the  
18 inhaler to ensure repeatable performance.

19 A brief description of the sequence of operation is as follows. A new well 244  
20 carrying the drug is advanced forward and positioned over the piezoelectric element  
21 254. A power switch 272 on the inhaler housing 212 (not shown in figure) is turned  
22 on. This connects the power source 274 to the electronics. At this point the output of  
23 the actuation controller circuit 270 is not enabled. When a minimum air-stream 250  
24 flowrate is established, the actuation controller 270 enables the vibrator driver circuit  
25 276 and the electrostatic voltage generator circuit 278. The high frequency vibrations  
26 set up by the piezoelectric vibrator 254 are coupled through the well 244 into the  
27 powder. These high frequency vibrations deaggregate the powder in the well and  
28 keep the powder in a fluidized state. The electrostatic plate 232 sets up an  
29 electrostatic field across the fluidized powder. The deaggregated particles, which  
30 carry an electrostatic charge, experience an electrostatic force and are lifted up by this

1 field set up by the electrostatic plate 232. This electrostatic force experienced by the  
2 charged particles is counteracted by the mass of the particles. Smaller particles which  
3 are unable to counteract their mass are lifted up toward the electrostatic plate 232,  
4 while larger size particles which cannot counteract their mass are left behind in the  
5 well 244. The voltage applied to the electrostatic plate 232 is selected so that only  
6 deaggregated drug particles, i.e. smaller size particles of choice, are lifted towards the  
7 electrostatic plate 232, where enter the air stream 250 and are carried to the  
8 mouthpiece 214. On the other hand, the electrostatic force on the charged particles is  
9 not so strong as to enable the particles to make it across the air stream 250 to the  
10 electrostatic plate 232.

11 The inner surface of the channel 215 and the passageway 234 is metalized and  
12 connected to ground. Without this metalization 236, static charges could build up on  
13 the inside surfaces of the channel 215 and passageway 234, and attract charged drug  
14 particles as they are lifted out of the well 244 and make their way to the mouthpiece  
15 214, thus reducing reproducibility of delivery from dose-to-dose of the inhaler.

16 Figure 11 shows a preferred schematic embodiment of the vibrator drive  
17 circuit 276. This configuration helps couple energy efficiency to the high frequency  
18 piezoelectric vibrator 254, while at the same time generating the necessary high  
19 voltages for driving the piezo. This circuit configuration enables the inhaler to be  
20 designed as a portable unit and enables it to achieve very small package dimensions  
21 relative to similar units described in the prior art. The circuit consists of an  
22 inductance 280 in series with a diode 284 and switch 288. The switch 288 may be of  
23 a bipolar transistor or a field effect transistor or any other means capable of switching  
24 at high frequency in an efficient manner, i.e. without loss of considerable energy.  
25 Elements 280, 284 and 288 are connected across a bypass capacitor 282 capable of  
26 carrying high frequency currents. The piezoelectric element 254 is connected across  
27 switch 288. The actuation controller 270 switches the switch 288 on and off at the  
28 appropriate frequency necessary to drive the piezoelectric vibrator. The sequence of  
29 operation is as follows: When switch 288 is turned ON, current builds up in the  
30 inductance 280. When switch 288 is turned OFF, the inductance 280 then resonates

1 with the internal capacitor of the piezo element 254. This series resonant circuit  
2 efficiently couples the energy stored in the inductance to the piezo element while at  
3 the same time generating the high voltage necessary to drive it. If necessary, the  
4 internal capacitance of the piezo may be supplemented by an external capacitor 286 to  
5 control the energy/voltage transfer characteristics to the piezo 254.

6 Figures 12A and 12B show the schematic representation of the electrostatic  
7 voltage generation circuit 278. The Figure 12A schematic is suitable for generating  
8 low voltages, for example, less than 200 volts. The actuation controller 270 turns a  
9 switch 296 ON and OFF at a frequency which will result in efficient build up of  
10 voltage across capacitor 294. When switch 296 turns ON, current builds up in an  
11 inductance coil 290. When switch 296 is turned OFF, the inductance pumps this  
12 energy into the output capacitor 294 by generating a voltage one diode drop higher  
13 than the output voltage. The inductor 290 continues to maintain this voltage till all  
14 the energy stored in it is transferred to capacitor 294. The electrostatic plate 232 is  
15 connected to capacitor 294. The voltage generated across capacitor 294 sets up the  
16 electrostatic field across the fluidized and deaggregated powder in the well 244.  
17 Capacitor 295 is a bypass capacitor for carrying the high frequency switching  
18 currents.

19 If a higher electrostatic field is required, it may be necessary to use the  
20 schematic shown in Figure 12B. Here a high frequency inverter 298 is coupled to a  
21 high frequency transformer 300. The output of transformer 300 feeds into voltage  
22 multiplier circuit 302 for stepping up the voltage to the required level. The output of  
23 the voltage multiplier circuit is connected to the electrostatic plate.

24 Figure 13 shows yet another embodiment 400 of the present invention. This  
25 embodiment would be suitable for those applications where we wish to further reduce  
26 the possibility of air turbulence picking up the partially deaggregated powder from the  
27 blister wells. This embodiment consists of a housing 402 which includes a  
28 mouthpiece 418 at one end of a main leg 408, and a main air inlet 416 at the opposite  
29 end of the leg 408. An opening 406 is provided at one end of a secondary leg 414 that  
30 opens into the main leg 408, and an air inlet 420 is provided at the opposite end of the

1 secondary leg 414. Housing 402 also includes a high frequency vibrator, such as  
2 piezoelectric vibrator 412, located in member 410 of the housing 402. A secondary  
3 channel 430 communicates with the secondary leg 414 at one end and a drug  
4 container 428 at the other end. Channel 430 allows the selected drug container to  
5 communicate with the secondary leg 414. Directly under the drug container is the  
6 vibrator 412.

7 The Figure 13 embodiment operates as follows: A new well 428 carrying the  
8 drug is advanced forward and positioned over the piezoelectric vibrator 412. A power  
9 switch on the inhaler housing (not shown in the figure) is turned on. This connects  
10 the power to the electronics. When the patient inhales a main air flow 405 and a  
11 secondary air flow 404 is established. The secondary air flow 404 causes a flapper  
12 valve 422 to open and enables the vibrator drive circuit 276 and the electrostatic  
13 generator circuit 278 (see Figure 10). The flapper valve functions as an air flow  
14 sensor. The high frequency vibrator 412 deaggregates the powder in the container  
15 428 and keeps it in a fluidized state. An electrostatic plate 424 sets up an electrostatic  
16 field across the fluidized powder. The deaggregated particles which carry a charge are  
17 lifted up towards electrostatic plate 424. The resulting particle stream 426 is  
18 introduced into the air stream 404 and is carried forward and introduced into the main  
19 air stream 405.

20 It will be appreciated that although the foregoing detailed description  
21 proceeded with reference being made to the preferred embodiments and methods of  
22 use, the present invention is not intended to be limited to these preferred embodiments  
23 and methods of use. Rather, the present invention is of broad scope and is intended to  
24 be limited only as set forth in the accompanying claims.

- 1           1. A dry powder inhaler comprising, a first chamber in which a dry powder  
2           may be deaggregated by means of a vibrator (36), a first air flow passageway (31) in  
3           which the deaggregated powder may be separated by size, and a second air flow  
4           passageway (26) in which the size-separated deaggregated powder may be picked up  
5           and carried for introduction into a patient.
- 6           2. An inhaler according to Claim 1, and further comprising at least one  
7           detector (40) for detecting velocity and/or pressure of air flow (F) in said passageway  
8           (26).
- 9           3. An inhaler according to claim 2, and further comprising a controller (70)  
10          adapted to automatically actuate or deactivate said vibrator (36) in response to signals  
11          from the detector (40).
- 12          4. An inhaler according to claim 3, wherein said controller (70) includes a  
13          user-actuable control for permitting a user to control actuation of said vibrator (36)  
14          based upon a selected type of powder.
- 15          5. In a dry powder inhaler comprising a chamber (234) in which a dry powder  
16          may be deaggregated by means of a vibrator (254), and an air flow passageway (250)  
17          in which the deaggregated powder picked up and carried for introduction into a  
18          patient, the improvement which comprises electrostatic potential means (232) for  
19          driving the deaggregated powder into the air flow passageway.
- 20          6. An inhaler according to claim 5, wherein at least a portion of the inner  
21          surface of the housing (215) of the inhaler is metallized (236).
- 22          7. An inhalation device, for dispensing of medication in a powder form,  
23          having a body (212) comprising an air outlet channel in said body portion providing a  
24          mouthpiece (214) for inhalation of air by the user;  
25                  a primary air inlet channel (216) in said body portion communicating with said  
26          air outlet channel;  
27                  a secondary channel (234) in said body portion communicating at one end  
28          thereof with said primary air inlet channel and said air outlet channel forming an air  
29          stream, and at its other end with supply (246) of said medication in powder form, a  
30          high frequency vibrator (254) for deaggregating the powder in said secondary channel

1 (234), and an electrostatic means (232) to separate by size the deaggregated powder in  
2 said channel and introduce the powder particles of size interest into the air stream.

3 8. An inhalation device according to claim 7, and comprising a high  
4 frequency inverter (298), a high frequency transformer (300) and a voltage multiplier  
5 circuit (302) for generating an electrostatic voltage for driving said high frequency  
6 generator (254).

7 9. An inhalation device according to claim 7, and further comprising an  
8 inhalation sensor (264) for activating said high frequency vibrator (254) in response to  
9 inhalation of air (250) by the user.

10 10. An inhalation device, for dispensing of medication in a powder form,  
11 having a body (402) comprising an air outlet channel in said body portion providing a  
12 mouthpiece (418) for inhalation of air by the user;

13 a primary air inlet channel (416) in said body portion communicating with said  
14 air outlet channel;

15 a secondary air inlet channel (414) in said body portion communicating with  
16 said air outlet channel;

17 a secondary channel (240) in said body portion communicating at one end  
18 thereof with said secondary air inlet channel and said air outlet channel forming a  
19 secondary air stream, and at its other end with a supply (428) of said medication in  
20 powder form, a high frequency vibrator (412) for deaggregating the powder, and an  
21 electrostatic means (422) to separate by size the deaggregated powder and introduce  
22 the powder particles of size interest into said secondary air stream (404).

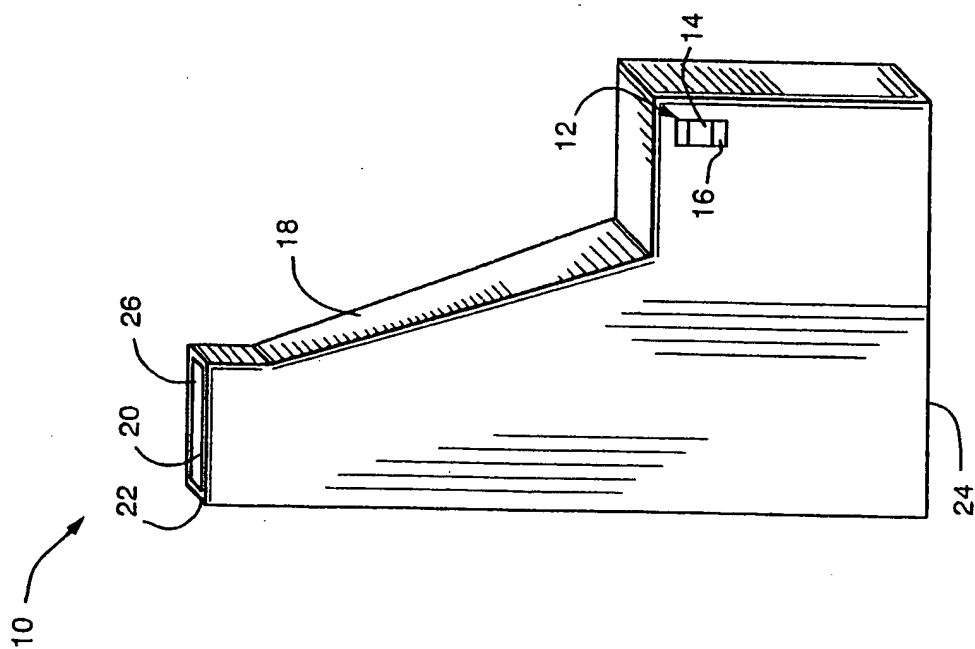


FIG. 1

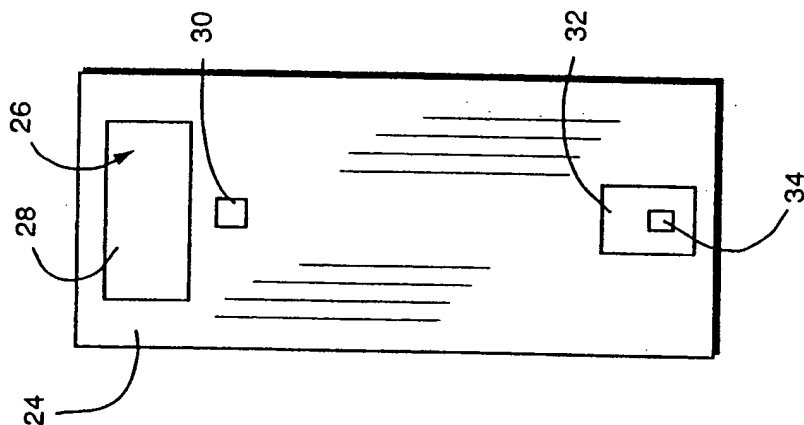


FIG. 2



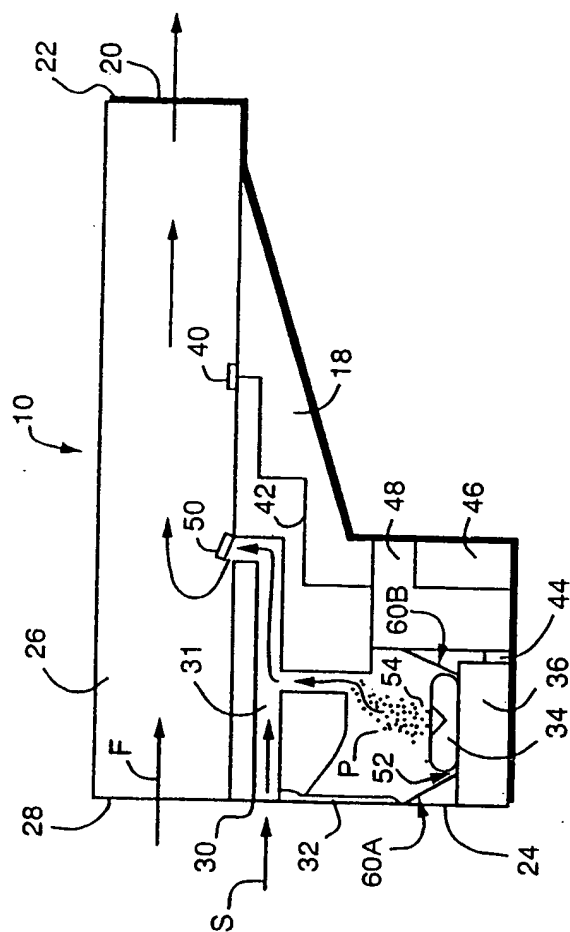


FIG. 3

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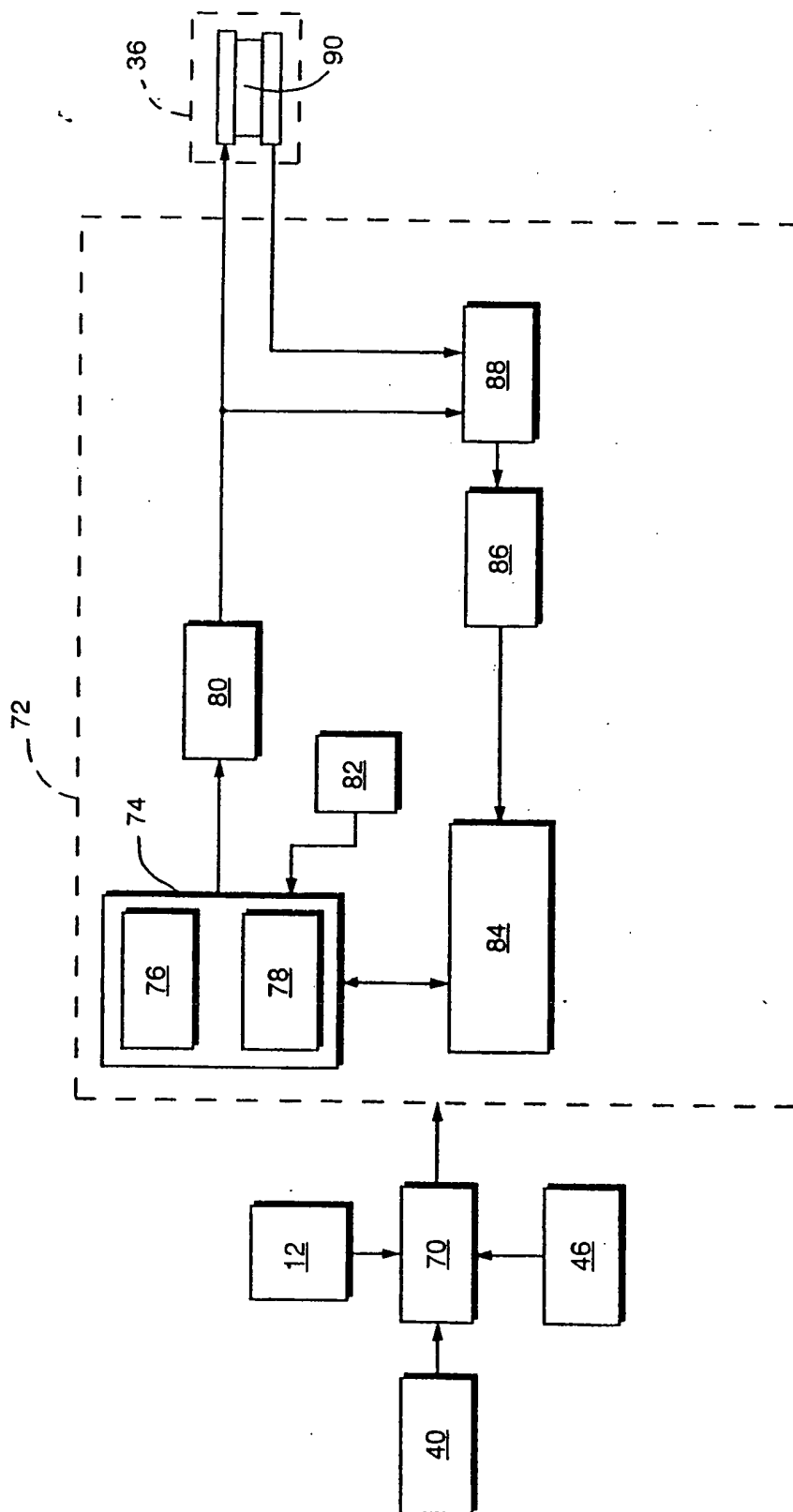


FIG. 4

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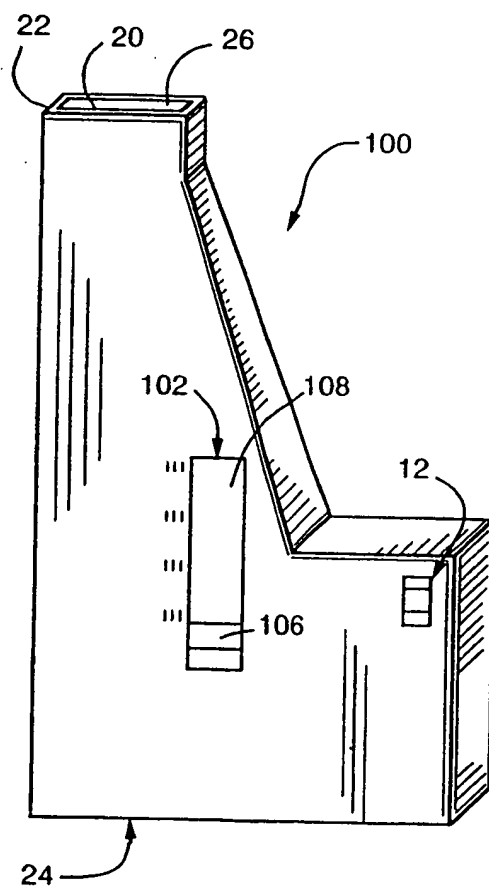


FIG. 5

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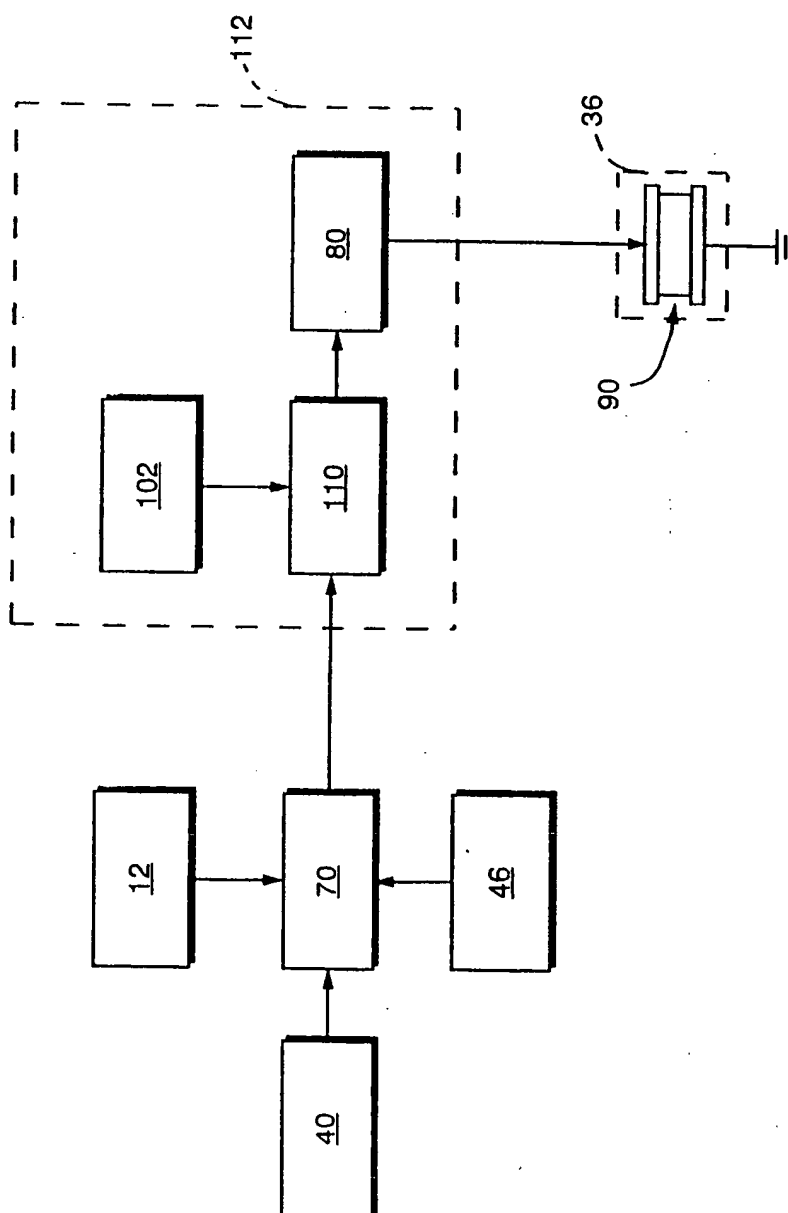


FIG. 6

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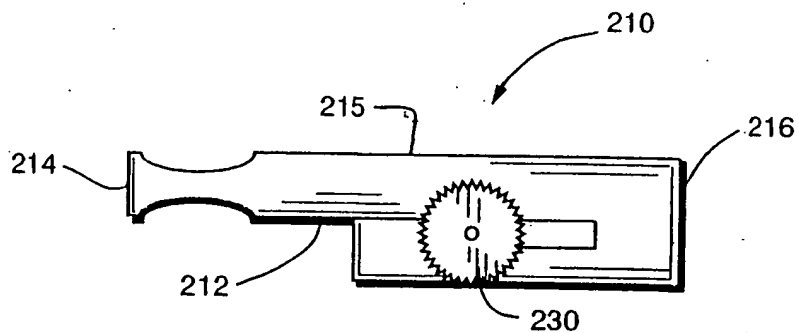


FIG. 7A

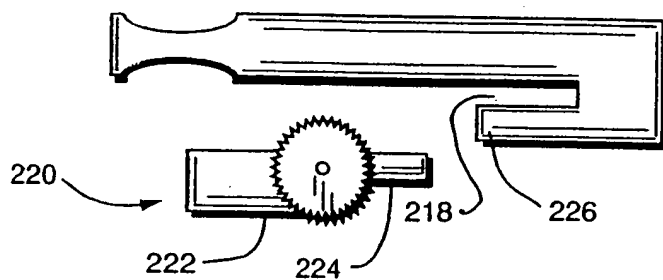


FIG. 7B

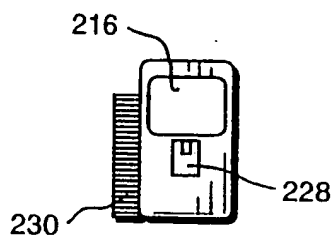


FIG. 8

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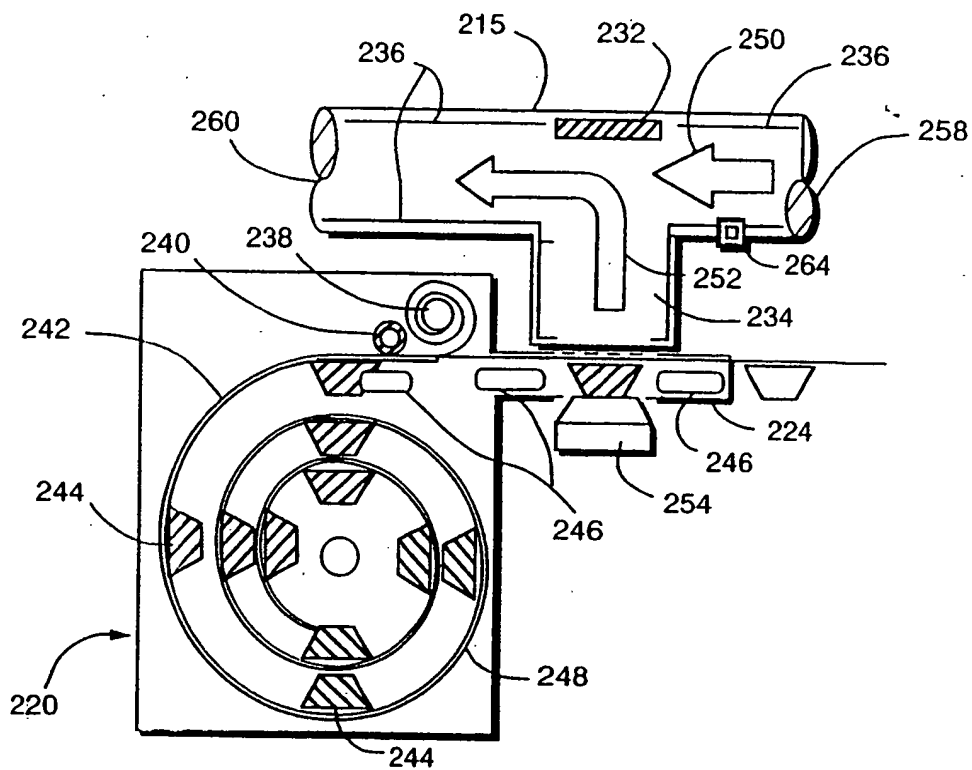


FIG. 9A

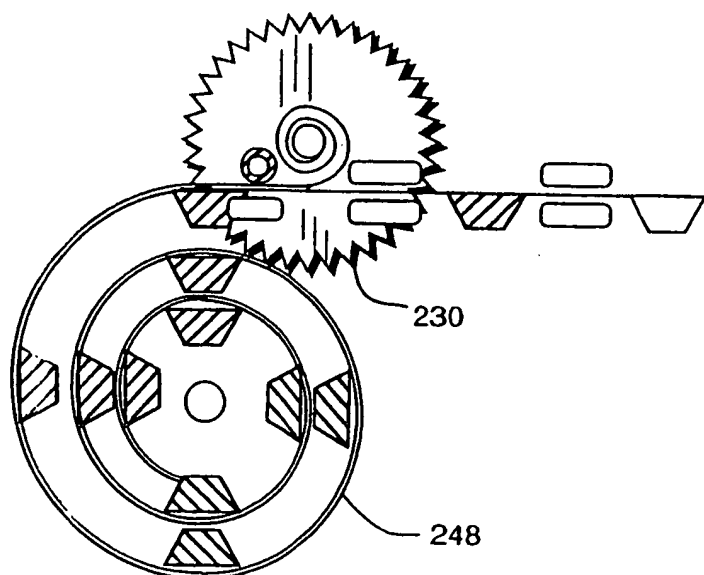


FIG. 9B

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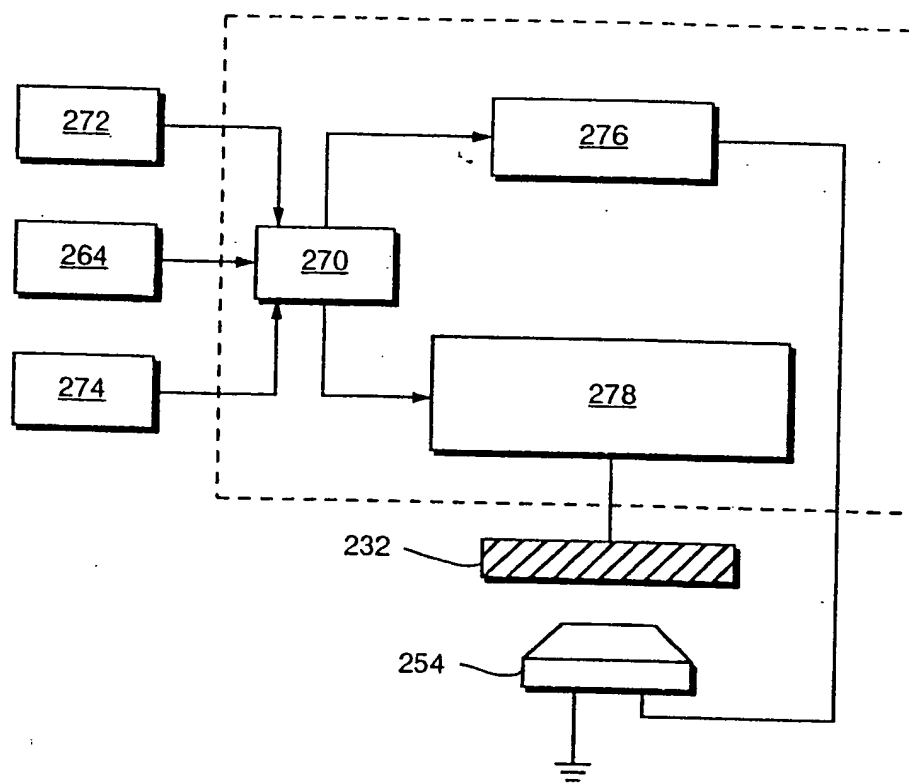


FIG. 10

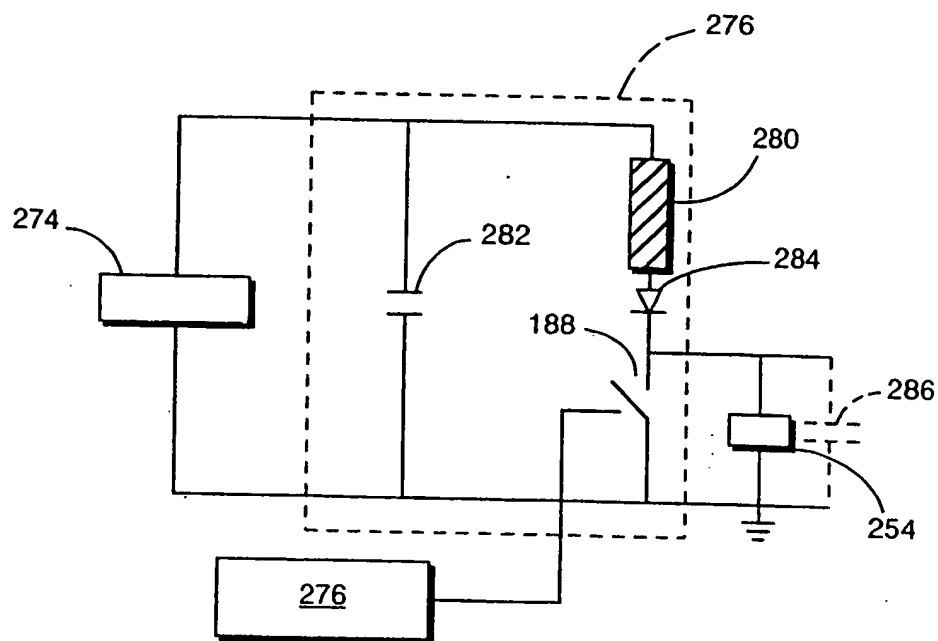


FIG. 11

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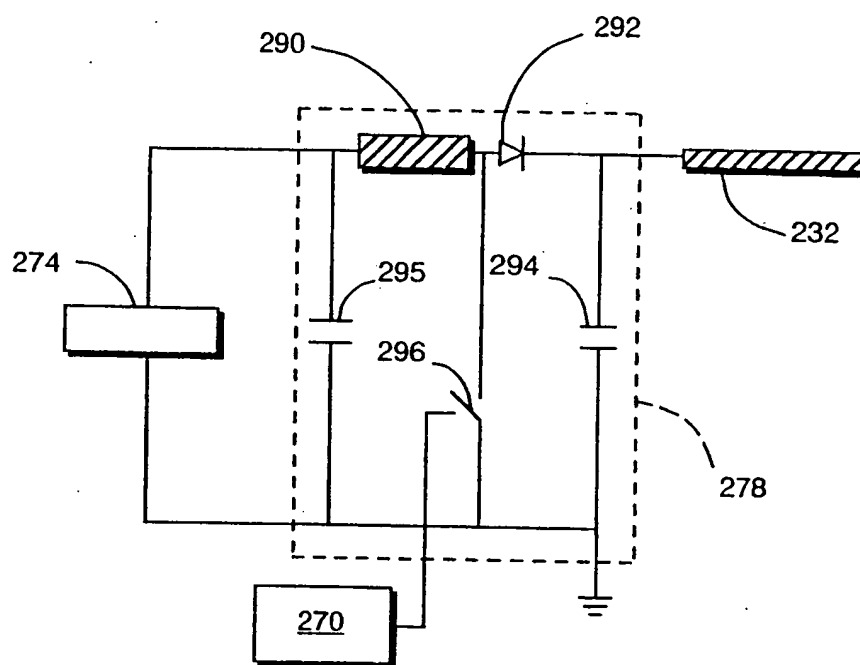


FIG. 12A

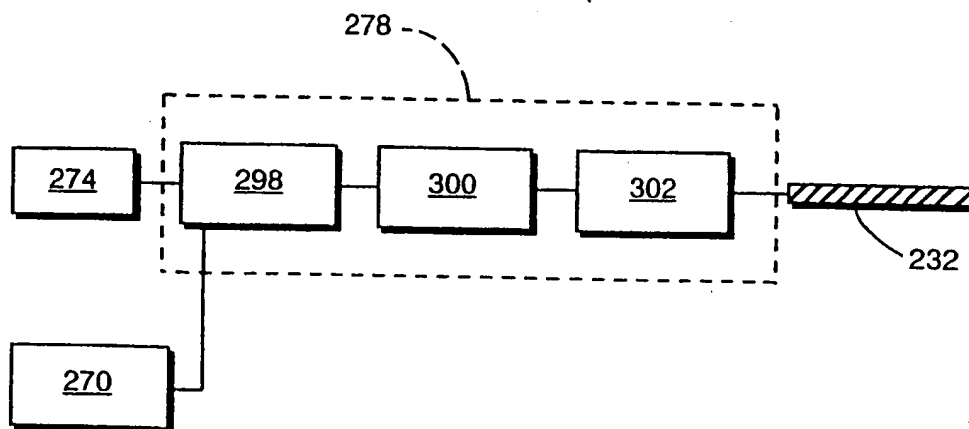


FIG. 12B



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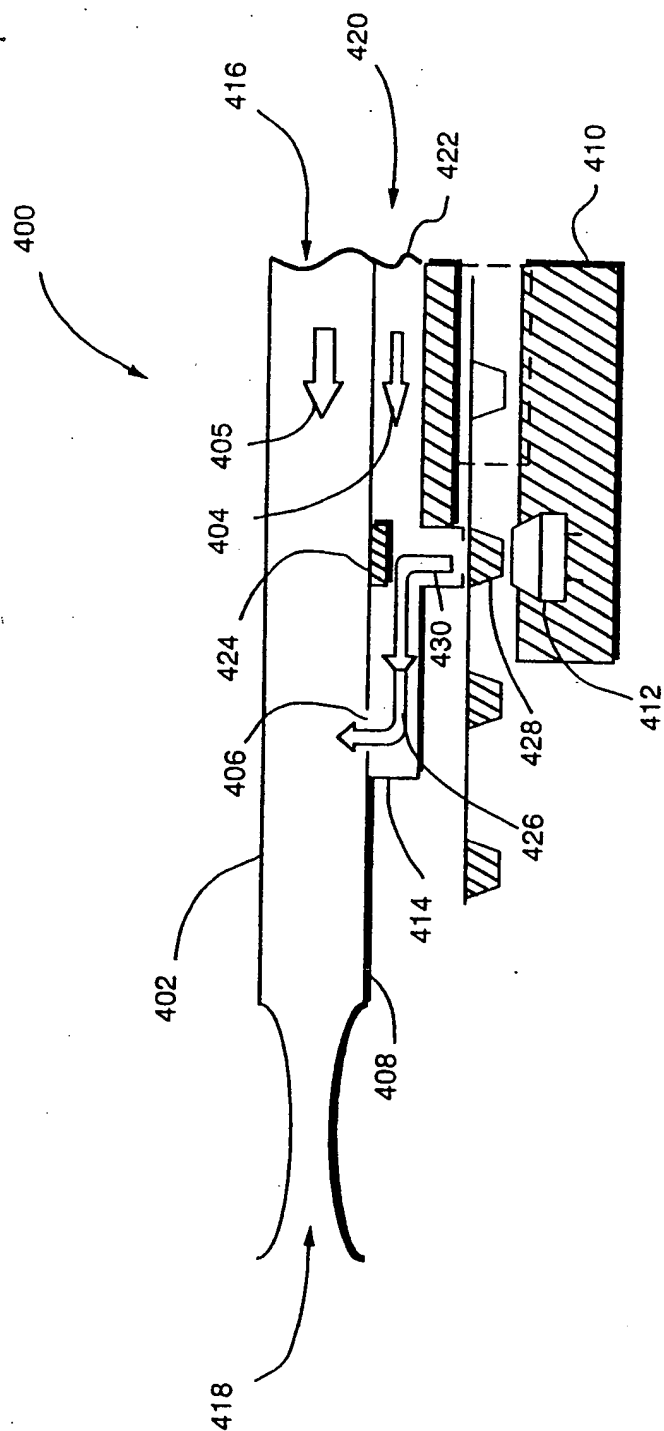


FIG. 13

## INTERNATIONAL SEARCH REPORT

International application No.

PCT/US97/08904

**A. CLASSIFICATION OF SUBJECT MATTER**

IPC(6) : A61M 15/00

US CL : 128/203.15, 200.16, 200.24, 203.12; 604/58

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 128/203.15, 200.16, 200.24, 203.12; 604/58

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

APS

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 3,948,264 A (WILKE ET AL) 06 April 1976, col. 2, lines 3-8; col. 3, lines 30 and 48; col. 4, lines 41-53.	1
Y	US 5,284,133 A (BURNS ET AL) 08 February 1994, col. 4, lines 40-41, cols. 8-12.	2-10
Y	US 5,522,383 A (CALVERT ET AL) 04 June 1996, col. 5, lines 18-48.	6
Y	US 5,469,843 A (HODSON) 28 November 1995, col. 4, lines 1-39.	5,7

☐ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	*T	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
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*L* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	*G*	document member of the same patent family
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Date of the actual completion of the international search

29 JULY 1997

Date of mailing of the international search report

29 AUG 1997

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